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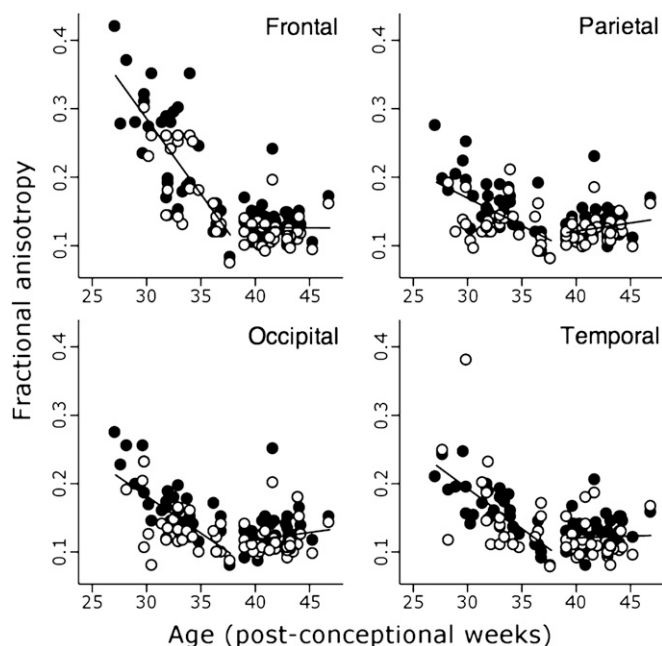
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**Fig. 1.** Regional changes in FA. Change in FA in cortical ROIs demonstrated by piecewise linear regression. ROIs were placed in gyri (black circles) and sulci (white circles) of frontal, parietal, occipital, and temporal cortex, and regression lines are shown for all samples. Note that FA is generally higher in the gyri in all four regions.

The decline in FA was reduced by longer exposure to extra-uterine life (Table S1), and FA was significantly higher in the 37 preterm infants imaged at term-corrected age than in 10 infants delivered at term after uncomplicated pregnancies (Fig. 3;  $P < 0.0001$ ). No dose-dependent effect of prematurity on the rate of change in MD was detected, but MD was also higher in preterm infants at term-corrected age than in term-born infants, although still falling rapidly (Fig. 3;  $P < 0.0001$ ).

In 39 preterm infants for whom the Griffiths' developmental quotient (DQ) was measured at around 2 y of age, higher DQ was related to more rapid changes in FA and in MD during the preterm period; however, after correction for multiple measurements, only the latter remained significant ( $P = 0.028$ ).

**Whole-Cortex Survey.** Images from 47 of the preterm cohort, including seven infants studied twice, were suitable for analysis using a method to survey changes in MD and FA across the whole cortex: gray matter-based spatial statistics, derived from tract-based spatial statistics (TBSS). Average FA at different ages during the preterm period is shown in Fig. 4A, and 4D maps of FA change over time are presented in [Movies S1](#) and [S2](#). Cortical voxels were grouped according to change in FA over time into three clusters, which provided the optimum representation of the data after repeated iterations of the *k*-means algorithm. The trajectories of FA change within each of the three clusters are shown in Fig. 4B, together with a randomly chosen set of 100 voxels per cluster to give a representation of the spread of the data. The anatomical locations of the clusters, which showed general but not complete hemispheric homology, are shown in Fig. 4C. In addition to these three clusters, a few voxels (6%) showed increasing FA trajectory, representing misclassified white matter, and were removed from the analysis.

Cortical trajectories of FA reproduced the biphasic pattern seen in the ROI analysis, with the decline in FA before 38 wk gestational age evident in clusters 2 and 3. Cluster 3 had the highest initial FA values and most rapid decrease; voxels with

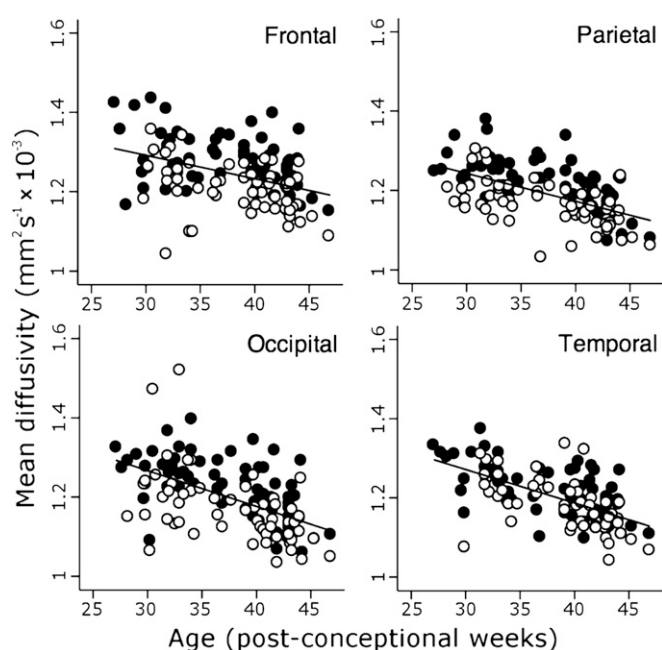
this time course were found predominantly in the frontal pole; superior and lateral parietal cortex; in the anterior temporal poles bilaterally; and in the left temporoparietal junction. Cluster 2 had a similar time course but with a lower initial FA value, and were widely distributed across lateral frontal, middle temporal, and lateral parietal cortices. FA in cluster 1 changed relatively little across the study period: these voxels were found predominantly in inferior frontal, medial occipital, and perirolandic cortex bilaterally, and right temporal regions.

Cortical MD was best described by a two-cluster model. MD at different ages is shown in Fig. 5A, and maps of MD change over time are presented in [Movies S3](#) and [S4](#). Fig. 5B shows the trajectory centers overlaid on 100 randomly sampled time courses, and cluster location is shown in Fig. 5C. MD decreased globally, with moderately higher values in cluster 1, located in superior, inferior frontal and prefrontal cortex, anterior temporal lobe, insula, and superior parietal cortex.

Localized measures of cortical growth were estimated by calculating the Jacobian determinants of the deformation fields that align the volumetric MR images to a population-based, spatio-temporal brain atlas. Growth varied across the cortex, but the average log-Jacobian in each of the clusters defined by FA trajectory showed a linear relation to the postconceptional age of the infant at imaging (Fig. 6 *A–C*). The rate of cortical growth was significantly related to the rate of FA change ( $P < 0.001$ ; Fig. 6*D*).

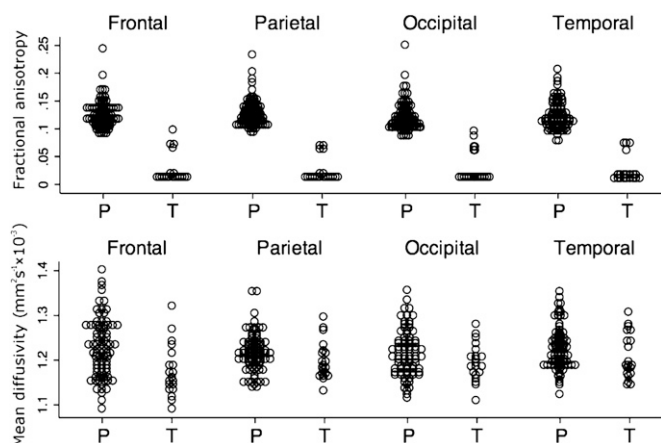
## Discussion

This spatiotemporal mapping of diffusion in human cerebral cortex from 27 to 46 wk postconception offers the opportunity of using millimeter-scale imaging data to infer the development of millimeter-scale neural organization across the whole cortex through reference to neuroanatomical data and diffusion–neuroanatomic correlations. Age-matched human neuroanatomic samples reveal the creation of an increasingly dense and complex cytoarchitecture during this period through dendritic arborization, glial proliferation, differentiation of radial glia, and synapse formation (18–21). Particular studies show that the length of basal dendrites,



**Fig. 2.** Regional changes in mean diffusivity. Change in MD in cortical ROIs demonstrated by linear regression. Data labeled as in Fig. 1. Note that MD is generally higher in the gyri in all four regions, and that in contrast to FA, the decline in MD continues after 38 wk of age.





**Fig. 3.** FA and MD at term-corrected age. FA and MD extracted from cortical ROIs were compared between all preterm infants imaged at term-corrected age (P;  $n = 37$ ) and a cohort of healthy, term-born controls (T;  $n = 10$ ). Cortical FA and MD were both significantly higher in the preterm infants at term in all regions.

dendritic spine density, and synapse number at term are lower in frontal association cortex than in primary sensory or motor regions (22, 23), and that the elongation of dendrites and the order of basal (but not apical) dendritic branching is complete at 38–40 wk postconception (24, 25). Microstructural maturation can also be altered by perinatal stress, which leads to the retraction of apical dendrites (26).

Direct diffusion–neuroanatomic correlations are difficult to acquire in human infants, and the data are few and only partially relevant (27). Fortunately, precise information is available from experimental studies. In developing rodents, the reductions of MD and FA colocalize and correlate with increased dendritic density and fewer nestin-positive radial glia (28); in ferrets, FA is

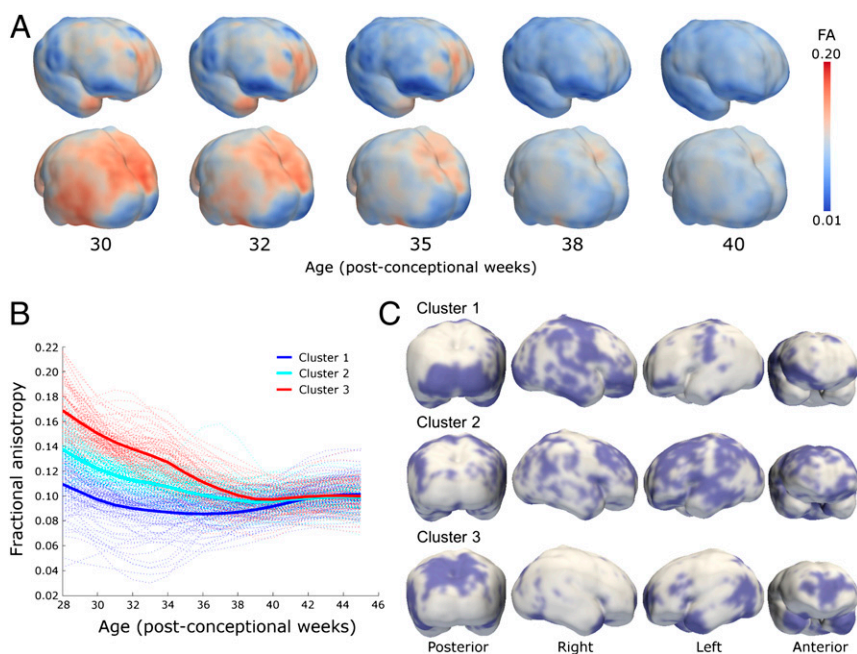
higher in regions with less-differentiated neurons and fewer orthogonal dendrites (29); and in preterm sheep, cerebral ischemia disrupts the normal maturational fall in cortical FA in proportion to a reduction in the complexity of the basal dendritic arbor of pyramidal neurons (30).

Many of the processes underlying mammalian cortical development are preserved across species (19). Though cross-species comparisons require caution, the consistency of the human and experimental data argues strongly that the observed diffusion changes are the consequence of neural growth and differentiation, with decreasing MD reporting growing tissue density secondary to increasing neurite number, cellular complexity, and synapse formation, and the fall in FA predominantly reflecting increasing dendritic elongation and branching orthogonal to cortical columns, particularly in the basal arbor. Other potential changes, such as differentiation of radial glia or retraction of apical dendrites, could also contribute but are likely to be quantitatively less significant.

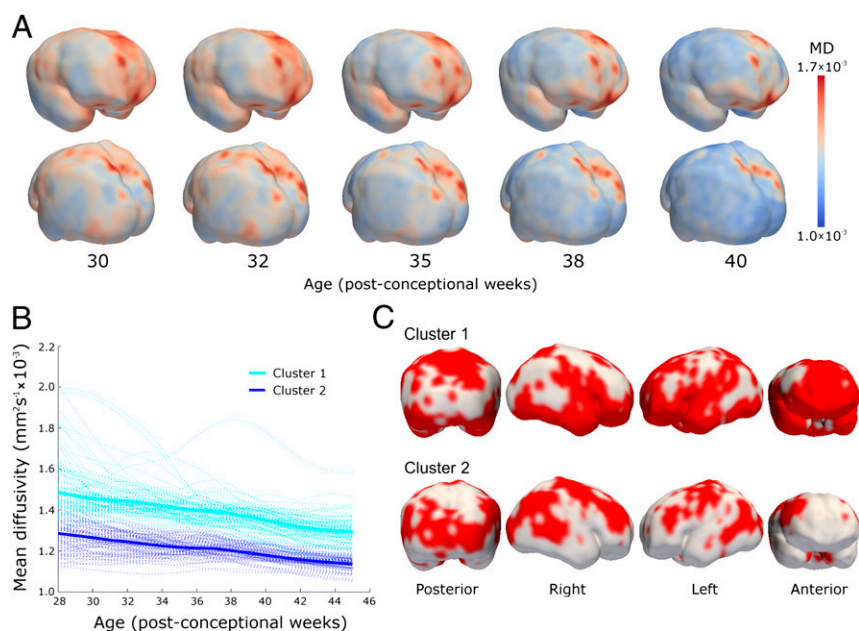
The current results are thus best understood as showing a consistent increase in cellular and synaptic complexity starting earlier in sulci than gyri, with rapid elongation of dendrites beginning in sulci and regions of early sulcation, then spreading into gyri and higher-order association cortex before slowing markedly after 38 wk postconception.

This complex microstructural development was impaired in a dose-dependent manner by premature exposure to the extra-uterine environment, and at term-corrected age, preterm infants showed significantly higher MD and FA than term-born controls. MD was still falling, consistent with ongoing increases in dendritic spine density and synaptogenesis (22, 31–33), but there was no suggestion of compensatory development in the aspects of dendritic arborization reflected by FA measurements. Gray matter-based spatial statistics may provide an appropriate method for further studies to determine whether differences persist.

The cortex-wide correlations between local developmental trajectories of FA and growth in cortical volume extend previous sample-based analyses and confirm the local synchronization of



**Fig. 4.** Global spatiotemporal mapping of changes in FA. (A) Cortical FA at five time-points during the preterm period mapped onto a smoothed isosurface representation of the population-based template image. (B) Cortical voxels were clustered into three groups according to the trajectory of change in FA over time. Kernel regression shows the developmental trajectory of FA in each cluster (thick solid lines) overlaid on 100 randomly sampled voxel time-courses from within each cluster (thin lines). (C) Cluster locations displayed on the same surface as A.



**Fig. 5.** Global spatiotemporal mapping of changes in MD. (A) Cortical MD at five time-points during the preterm period. (B) Cortical voxels were clustered into two groups based on the trajectory of MD change over time. Kernel regression shows trajectory of group-average MD in both clusters (thick lines) overlaid onto 100 randomly sampled voxel time courses (thin lines). (C) Cluster locations are displayed as in Fig. 4.

microscopic and macroscopic maturation (34). This program may also coordinate with the growth of functional connectivity, because the regions with most rapid development are predominantly higher-order association areas that are engaged by functional networks, such as the executive and default mode systems, which show greater changes than primary auditory or visual networks during this period (35).

The rate of cortical growth and maturation was rapid during the studied period, and predicted neurodevelopmental test scores in later childhood (36, 37). Development was most rapid in the frontal pole, which stands at the apex of the prefrontal hierarchy, engaged in goal-setting and monitoring (38); the temporal pole, involved in social and emotional processing (39); and the parietal association cortex, critical for working memory and visual-spatial processing (40). These functions are frequently specifically impaired in children born preterm, consistent with the hypothesis that rapid microstructural growth confers vulnerability to the effect of premature extrauterine life.

These results suggest a mechanism for the reduced cognitive abilities in preterm infants; demonstrate the importance of brain development in the late preterm period; and may help account for the adverse effects of even minor degrees of prematurity (41).

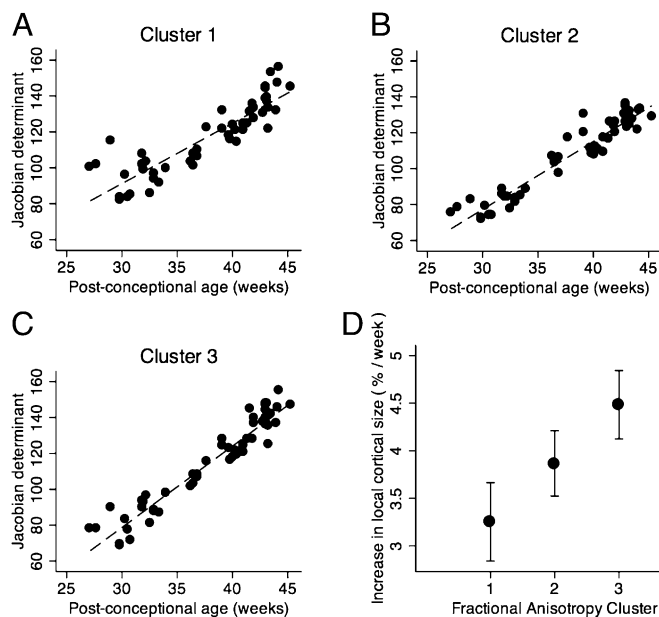
## Materials and Methods

**Subjects.** The study was approved by the Hammersmith Hospital Research Ethics Committee, and infants were recruited after written informed parental consent. Clinical information for the preterm cohort is given in [SI Materials and Methods](#) and [Table S3](#). No infants had evidence of cystic periventricular leukomalacia or hemorrhagic parenchymal infarction on conventional MRI.

**Image Acquisition.** Fifteen-direction DTI and T2-weighted MRI was performed on a Philips 3.0 Tesla system using an eight-channel phased-array head coil. MR procedures are described in detail in [SI Materials and Methods](#).

**ROI Analysis.** DTI data were processed using DTI Studio version 2.1 (42). Diffusion tensors were estimated voxel-wise to create FA and MD maps. Multiple ROIs were manually delineated in ~8–10 axial slices of the MD maps, depending on the maturity of the brain. Each slice had 10–20 regions delineated on both cortical gyri and sulci bilaterally of all four cortical lobes: frontal, parietal, occipital, and temporal (Fig. S1).

**Investigation of Partial-Volume Effects.** To analyze possible partial-volume effects of cerebrospinal fluid on measurements, three infants at 26 wk, 34 wk, and term-equivalent age were subject to an additional diffusion fluid-attenuated inversion recovery, or FLAIR, sequence during the same acquisition. The influence of partial-volume effects on diffusion measures was tested (*SI Materials and Methods*; Fig. S1) and no evidence of significant contamination was found.



**Fig. 6.** Parallel microstructural development and macrostructural growth in the cortex. The relation between increasing cortical volume, represented by the log-Jacobian determinant, and postconceptional age in voxels clustered by spatiotemporal mapping of cortical FA (A, cluster 1; B, cluster 2; C, cluster 3; location of clusters shown in Fig. 4). Rate of change of volume over time was significantly different in each cluster (D).

**Statistical Modeling.** Stata 12.1 (StataCorp) was used for all statistical analyses. To account for repeated sampling in some individuals, we used generalized least-squares regression to create parallel models of the rate of change in FA and MD values. The effects of postconceptional age, length of extrauterine life, brain region, sulcus or gyrus, total brain volume, and their interactions were examined in a series of regression models, and the most informative model chosen using the Akaike and Bayesian information criteria; these included the postconceptional age, brain region, gyrus or sulcus, and length of extrauterine life as main effects alongside the interactions between postconceptional age and the other variables. The selected models were tested by inspecting histograms of idiosyncratic and subject-specific errors and normal quantile (Q-Q) plots; these showed adequate fitting but disclosed outliers that were removed with change to inferences. Stability was analyzed using perturbation analysis, adding random values to variables and reestimating the model 200 times.

Inspection of the raw data showed nonlinear changes in FA over time and we therefore tested models based on first- and second-order polynomials and biphasic linear piecewise regression with a node placed at 38 wk postconception. Both polynomial and piecewise methods produced appropriate models, but perturbation analysis showed relative instability in the polynomial regression, and biphasic piecewise analysis was used for analysis. MD was less obviously biphasic, and information criteria favored the monophasic model, which we report; however, the results for mono- and biphasic regressions were broadly similar, though the differences between gyri and sulci were less, and the effect of prematurity more, significant in the biphasic analysis. Post hoc Wald tests were used to determine where significant differences existed between rate of change in each brain region and across time periods (pre- and post-38 wk).

To confirm the effect of prematurity, we compared preterm infants imaged at term-corrected age with 10 term-born control subjects using analysis of variance, with age at scan, brain region, gyrus or sulcus, and subject group (preterm/control) as main effects.

**Neurodevelopmental Outcome.** Infants in the study were offered entry into a follow-up program. At ~2 y corrected age, 39 subjects undertook the Griffith Mental Developmental Scales, which provide an overall DQ made up of locomotor; personal and social; hearing and language; eye-hand coordination; and performance subscales. The relation of DQ to changes in FA and MD were tested, and the contributions of the component subscales explored by linear regression. To aid interpretation of main effects, data were demeaned and models were corrected for multiple measurements from each individual.

**Voxel-Wise Analysis.** Fifty-four images were included for voxel-wise analysis after ensuring both that T2-weighted structural MRI and DTI were free from artifacts that would preclude computational processing and alignment to the template space of all images was accurate. The subset did not significantly differ from the full cohort in age at birth or at imaging.

**Image Processing.** We describe a unique method for aligning cortical data from multiple subjects into a common space to provide a voxel-wise spatial characterization of FA and MD change across the whole cortex.

To resolve regional differences in cortical anisotropy, it is necessary to align anatomically correspondent regions across individuals. To mitigate the confounding effects of anatomical misalignment between subjects and to remove partial-volume contamination due to the arbitrary choice of smoothing kernel often used in such analyses, we adapt a well-known processing pipeline for diffusion data designed to overcome such issues, TBSS (43), to generate gray matter-based spatial statistics for use in cortical analysis.

Image processing was performed with FSL (version 4.1.9) (44), and the processing pipeline is illustrated in Fig. S2. Diffusion datasets were corrected for distortion due to eddy currents, and FA and MD maps were constructed. Nonlinear registration (using the IRTK software package, [www.doc.ic.ac.uk/~dr/software/](http://www.doc.ic.ac.uk/~dr/software/)) (45) was used to align each infant's non-diffusion-weighted ( $b = 0$ ) image to their corresponding T2-weighted structural image. T2 volumes were bias corrected and segmented into three tissue classes (cortex, white matter, cerebrospinal fluid) using FAST ("FMRIB's Automated Segmentation Tool," Functional MRI of the Brain Centre, Oxford, UK) and age-appropriate anatomical priors (46). Nonlinear image registration was used to align each T2 image to a population-based template at a time-point close to the mean age of the group at the time of imaging (gestational week 36). Registration was performed in two steps, first to an age-appropriate T2 template within a population-based, spatiotemporal atlas (46), followed by longitudinal

registration toward to the final 36-wk template (47). Probabilistic cortical tissue maps were inspected and transformed to the common template space alongside FA and MD maps (via the intermediate T2 image).

A mean cortical map was produced by merging the aligned cortical probability maps, and skeletonized to retain only a core of highly probable cortical voxels as a thin curved surface at the center of the cortex. Individual cortical measurements were then projected onto the cortical skeleton; this was achieved by searching in a direction perpendicular to the cortical skeleton identifying maximally probable cortical voxels in each of the spatially transformed cortical probability maps, such that only data from nearby voxels with maximal cortical probability were kept and projected onto the skeleton. FA and MD data from the identified cortical voxels were then projected onto the skeleton for analysis. In contrast to TBSS, data projection was based not on aligning voxels with high FA, because FA was expected to vary dramatically across the cohort. Instead, voxels with high probability of containing gray matter were sought, thus ensuring that only diffusion measures from cortical voxels were analyzed. To further remove the possibility of analyzing voxels that did not contain FA data due to misregistration of individual subjects' diffusion and T2 images, voxels with a mean value across the whole group of less than 0.005 were excluded from the analysis.

**Spatial Characterization of Microstructural Change.** Skeletonized cortical voxels were grouped according to the trajectory of change in FA and MD across the cohort using a combination of kernel regression and unsupervised clustering.

Because the ages of the subjects were irregularly scattered over the time interval studied, kernel regression was applied to generate, for each voxel, group average measurements of FA at a regular sequence of time points.

Let  $y_{is}$  denote the measurement at voxel  $i$  for subject  $s$ ; let  $a_s$  represent the age of subject  $s$ . The kernel regression estimate for the value at age (time)  $t$  for voxel  $i$  is given by

$$y_i(t) = \frac{1}{z} \sum_s y_{is} \exp(-(t - a_s)^2 / \kappa^2).$$

The width parameter,  $\kappa$ , was chosen so that the kernel's full width at half-maximum was 4 wk, and  $z$  is a normalizing constant. A sequence of regularly spaced ages (values of  $t$ ) at 1-wk intervals over the age range is denoted by  $\{t_k\}$  for  $k = 1, \dots, K$  and the vector  $\mathbf{y}_i = (y_{i1}, \dots, y_{iK})^T$  represents the measurements at voxel  $i$  for the regular time points  $\{t_k\}$ .

The set of all time-regularized vectors  $\{\mathbf{y}_i\}$  for  $i = 1, \dots, N$ , where  $N$  is the total number of voxels, was grouped into clusters using  $k$ -means; this provides  $C$  cluster centroids  $\mu_1, \dots, \mu_C$  such that each voxel is assigned to the cluster with the nearest Euclidean distance, i.e., the cluster label assigned to voxel  $i$  is  $z_i$ ,  $1 \leq z_i \leq C$ , where  $z_i = \arg \min_z (\mathbf{y}_i - \mu_z)^2$ . The  $k$ -means algorithm is an iterative stochastic method that is initialized with randomized estimates for the trajectory centers and is run to convergence multiple times. Ten repeated starts were used with the initial estimates derived from a random subsample of 10% of the voxels. The whole process was repeated, varying numbers of clusters, and the final number of clusters for each type of data was selected to be the largest for which no empty clusters were generated during the iterations of the algorithm.

**Macrostructural Development over Time.** Using the method described above, maps of relative volume change were calculated in the form of the Jacobian determinant of the transformation aligning each T2 image to the population-based template image. These values were projected onto the mean cortical skeleton from high-probability cortical voxels in an analysis analogous to deformation (or tensor)-based morphometry (45, 48). Logarithms of voxel-wise Jacobian values were calculated, averaged over every voxel within a cluster, and the rate of change of volume over the age interval compared between clusters with multivariate regression. Outliers were assessed by inspection of Cook's distance, and dropped if the value was greater than 0.2. A post hoc Wald test was used to test for differences between slopes.

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